

Research Paper

Microspheres with Ultrahigh Holmium Content for Radioablation of Malignancies

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Purpose. The aim of this study was to develop microspheres with an ultra high holmium content which can be neutron activated for radioablation of malignancies. These microspheres are proposed to be delivered selectively through either intratumoral injections into solid tumors or administered via an intravascularly placed catheter.

Methods. Microspheres were prepared by solvent evaporation, using holmium acetylacetonate (HoAcAc) crystals as the sole ingredient. Microspheres were characterized using light and scanning electron microscopy, coulter counter, titrimetry, infrared and Raman spectroscopy, differential scanning calorimetry, X-ray powder diffraction, magnetic resonance imaging (MRI), and X-ray computed tomography (CT).

Results. Microspheres, thus prepared displayed a smooth surface. The holmium content of the HoAcAc microspheres (44% (w/w)) was higher than the holmium content of the starting material, HoAcAc crystals (33% (w/w)). This was attributed to the loss of acetylacetonate from the HoAcAc complex, during rearrangement of acetylacetonate around the holmium ion. The increase of the holmium content allows for the detection of (sub)microgram amounts of microspheres using MRI and CT.

Conclusions. HoAcAc microspheres with an ultra-high holmium content were prepared. These microspheres are suitable for radioablation of tumors by intratumoral injections or treatment of liver tumors through transcatheter administration.

KEY WORDS: holmiumacetylacetonate; intratumoral; microspheres; multimodality; radioablation.

INTRODUCTION

Worldwide, primary liver cancer (hepatocellular carcinoma or cholangiocarcinoma) is the sixth most common cancer, and each year over 600,000 new cases are presented. A limited number of patients is eligible for surgical resection (partial hepatectomy or liver transplantation), limiting the 5 year survival rate to only 3–5% (1,2). The use of systemic

chemotherapy has been proven ineffective, however recently a survival benefit of several months has been reported for the oral multikinase inhibitor sorafenib (3).

The liver is also a common site of metastasis, and more than 50% of patients with primary malignancies will develop hepatic metastases. A very common type of cancer to metastasize solely to the liver is colorectal carcinoma. Each year over 1,000,000 new cases of colorectal cancer are presented and the mortality is approximately 500,000 patients per year. Five year survival of patients in the developed world with colorectal cancer is approximately 55%, with main prognostic factors being the extent of lymphatic spread, the number and resectability of liver metastases (1,2). Surgical resection, considered to be the only curative treatment option, is only eligible in 10% to 20% of patients (4). Currently applied chemotherapy protocols (e.g. FOLFOX or FOLFORI, 5-fluorouracil/leucovorin combined with oxaliplatin or irinotecan, respectively, in combination with the angiogenesis inhibitor bevacizumab) are associated with a survival of patients with unresectable liver metastases of nearly 2 years (5,6).

Intra-arterial radioembolisation with radioactive microspheres (glass- or resin-based) containing the high-energy beta emitter yttrium-90 (⁹⁰Y) is currently increasingly applied in patients with unresectable hepatic malignancies. This ⁹⁰Y radioembolisation treatment has shown very high response

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rates (up to 91%), in both salvage setting and as a first-line treatment option (7,8). The lack of (quantitative) imaging options for ^{90}Y (9) has led to the development of holmium-166 loaded poly(L-lactic acid) ($^{166}\text{HoPLLA}$) microspheres, since ^{166}Ho emits gamma rays and beta particles that can be used for nuclear imaging and therapy, respectively (10–12). Moreover, holmium is highly paramagnetic and has a high linear attenuation coefficient allowing for visualization by magnetic resonance imaging (MRI) and X-ray computed tomography (CT), respectively (13,14).

Unfortunately, restrictions to inclusion to this intra-arterial transcatheter radioembolisation approach exist. For example, in patients who have been heavily pretreated with bevacizumab or cetuximab, the tumor feeding vessels may be too feeble for the microspheres to be deposited peri- and endotumorally (15). Efficacy may also be diminished in patients with hypovascular liver tumors. Furthermore, patients with portal vein thrombosis are excluded from treatment with the resin microspheres (16). Extensive liver cirrhosis and poor general health may also hamper the use of this treatment option.

Especially in patients with a limited number of unresectable intrahepatic tumors, not eligible for transcatheter radioembolisation, intratumoral injections of radioactive microspheres might be an option. This approach has been explored in patients with liver tumors using ^{90}Y glass microspheres, showing a response rate in 90% of patients (17). Direct intratumoral injection requires small deposits of radioactive microspheres in compact tumor tissue, limiting the overall injection volume to 0.1–0.3 ml (17,18). Consequently, the amount of activity per injection should be very high.

The purpose of this study was to prepare holmium loaded microspheres, using holmium acetylacetonate (HoAcAc) crystals as the sole starting material, without the use of PLLA as matrix forming polymer, to increase the content of holmium per sphere in order to obtain microspheres suitable for intratumoral application.

MATERIALS AND METHODS

Materials

All chemicals are commercially available and were used as obtained. Acetylacetone (2,4-pentanedione, AcAc ; >99%), ammoniumhydroxide (NH_4OH ; 29.3% in water), chloroform (HPLC-grade), phosphorus pentoxide (Sicapent®), polyvinyl alcohol (PVA, average MW 30,000–70,000) and Pluronic F68® ($\text{PEO}_{100}\text{PPO}_{65}\text{PEO}_{100}$; MW 9,840–14,600) were purchased from Sigma Aldrich (Steinheim, Germany). Holmium CertiPUR ICP standard and hexamethylentetramine were purchased from Merck (Darmstadt, Germany). Seakem LE Agarose was purchased from Lonza (Basel, Switzerland). Holmium (III) chloride hexahydrate ($\text{HoCl}_3 \cdot 6\text{H}_2\text{O}$; 99.95%) was purchased from Metall Rare Earth Ltd (Shenzhen, China).

Preparation of HoAcAc Microspheres

The holmium acetylacetonate microspheres (HoAcAc MS) were prepared using a solvent evaporation process. Holmium acetylacetonate crystals were prepared as previously described by Nijssen *et al.* (10). HoAcAc crystals were

dissolved in chloroform (186 g, 5.5% (*w/w*)) and emulsified in an aqueous PVA solution (1 l, 2% (*w/w*)). The chloroform/water emulsion was continuously stirred at a preset stirring speed (300–500 rpm). To evaporate chloroform, the mixture was thermostated at 25°C and a constant flow of nitrogen (12 l min^{-1}) was applied. After 40 h of evaporation the formed microspheres were collected by centrifugation and washed five times with water. The washed microspheres were sieved using an electronic sieve vibrator, (EMS 755) and ultrasonic processor (UDS 751; Topaz GmbH, Dresden, Germany) as described by Zielhuis *et al.* (19). The microspheres were dried at room temperature for 24 h, followed by drying at 50°C for 48 h.

Size Distribution, Holmium Content and Surface Characteristics

The size distribution of the sieved fractions and dried fractions was determined using a Coulter counter (Multisizer 3, Beckman Coulter, Mijdrecht, The Netherlands), equipped with an orifice of 100 μm .

The holmium content of the microspheres was determined by complexometric titration with EDTA as described by Zielhuis *et al.* (19), and Inductively Coupled Plasma Optical Emission spectroscopy (ICP OES). Samples were measured at three different wavelengths (399.989; 345.600 and 347.426 nm) in an Optima 4300 CV (PerkinElmer; Norwalk, USA).

Elemental analysis of carbon, hydrogen, oxygen and holmium of the HoAcAc crystals and HoAcAc microspheres was performed by H. Kolbe, Mülheim an der Ruhr, Germany.

SEM micrographs were acquired using a FEI PHENOM (FEI Company, Eindhoven, The Netherlands) electron microscope. Samples were mounted on an aluminum stub, and coated with a Pt layer of 6 nm.

Raman Spectroscopy

Raman spectroscopy was performed on a Kaiser RXN spectrometer equipped with a 70 mW 785 nm diode laser for excitation, a holographic grating for dispersion and a Peltier cooled Andor CCD camera for detection.

Differential Scanning Calorimetry

Modulated Differential Scanning Calorimetry (mDSC) measurements were performed using a DSC Q1000 (TA Instruments Inc., New Castle, DE, USA). The modulation amplitude was set at 1°C min^{-1} . Samples were heated from 20°C to 220°C with a heating rate of 2°C min^{-1} .

X-ray Diffraction

X-ray diffraction patterns were obtained on a Nonius κ -CCD diffractometer, with a sealed tube using $\text{MoK}\alpha$ radiation with a graphite monochromator. Powder patterns were recorded to a maximum scattering angle (2θ) 22°. The samples were contained in boroglass capillaries.

Neutron Activation

Neutron activation was performed in the pneumatic rabbit system operational at a research reactor facility (Department of Radiation, Radionuclides and Reactors, Delft University of Technology, Delft, The Netherlands). Samples were irradiated for 3 or 6 h with a thermal neutron flux of $5 \times 10^{12} \text{ n cm}^{-2} \text{ s}^{-1}$. The radioactive ^{166}Ho was left to decay for 1 month, to ensure safe handling of HoAcAc microspheres.

Multimodality Imaging Characteristics

To determine the sensitivity of MRI and CT for the HoAcAc microspheres, phantom experiments were carried out on MRI and CT. The phantom used to determine MRI and CT sensitivity consisted of agarose (2% (w/w)) gel samples in which HoAcAc microspheres were homogeneously dispersed (loadings ranged from 0 to 4 mg microspheres per ml agarose) in plastic tubes (diameter 10 mm, length 100 mm). MR imaging was performed using a 1.5 T clinical MR scanner (Intera, Philips Medical Systems, Best, The Netherlands). To determine the r_2^* relaxivity, which represents the MR sensitivity of the HoAcAc microspheres, transverse images were made using a multiple gradient echo MR sequence with 15 echos, an echo spacing of 1.39 ms a repetition time of 500 ms, a field of view (FOV) of 128 mm, a voxel size of $1 \times 1 \times 10 \text{ mm}$, two signal averages and a 60° flip angle. Monoexponential signal decay was assumed. Data processing was performed as described by Seevinck *et al.* (14). A second agarose gel phantom was constructed for qualitative imaging. This gel consisted of 2% (w/w) agarose, with pockets for the administration of a suspension of HoAcAc microspheres to obtain depots of 1 μg to 1 mg. The imaging parameters were similar to the imaging parameters mentioned before, except for the slice thickness, which was 1 mm.

To mimic potential *in vivo* imaging applications, depots of HoAcAc microspheres were injected in an *ex vivo* rabbit liver. The excised liver was flushed with water, and placed in an aqueous solution containing MnCl_2 (19.2 mg/L), to reduce the relaxation time of the water. Fifty microlitre of a suspension of HoAcAc microspheres was administered to the liver, to obtain depots of 1, 5 and 10 μg microspheres. The imaging parameters were similar to the imaging parameters

mentioned before. For the MR images displayed in Fig. 5A, D, E and F an echo time of 20 ms was used.

Quantitative X-ray CT imaging was performed on a clinical 64 slice CT scanner (Brilliance, Philips Medical Systems, Best, The Netherlands). The sample tubes were positioned co-axially to the main axis of the scanner. Using the methods described by Seevinck *et al.*, a linear regression curve was constructed to determine the sensitivity of X-ray CT for HoAcAc microspheres (14).

RESULTS AND DISCUSSION

Size Distribution, Holmium Content and Surface Characteristics

We found that HoAcAc microspheres could be obtained of HoAcAc crystals without using PLLA as a matrix forming polymer using a solvent evaporation technique.

The size distribution, surface morphology of the microspheres were characterized using Coulter Counter, light microscopy and scanning electron microscopy (SEM), both before and after neutron activation. The particle size distribution was rather broad, from 5 to 40 μm , with an average microsphere size of 15 μm when the microspheres were prepared at 500 rpm. The average particle size could be tailored by altering the stirring rate during emulsifying and increased from 15 μm at 500 rpm to 20 μm at 400 rpm and 26 μm at 300 rpm. The size distribution should be narrow to control the biodistribution of the microspheres and to reduce possible shunting of small microspheres to non-target organs after administration. Therefore, a sieving step is necessary to obtain a more confined size distribution. More than 93% of the microspheres had a size between 15–20 μm after sieving. No changes in microsphere size distribution were observed after neutron activation, which is an indication that small fragments due to radiation damage were absent. Light and scanning electron microscopy showed that spherical particles with a smooth surface were formed (Fig. 1A and B). Neither surface damage nor agglomeration was observed after neutron activation of the microspheres. After neutron activation for 3 or even 6 h, the surface of the microspheres only showed small crevices. However, no large fragments were present (Fig. 1C). This, in combination with the size

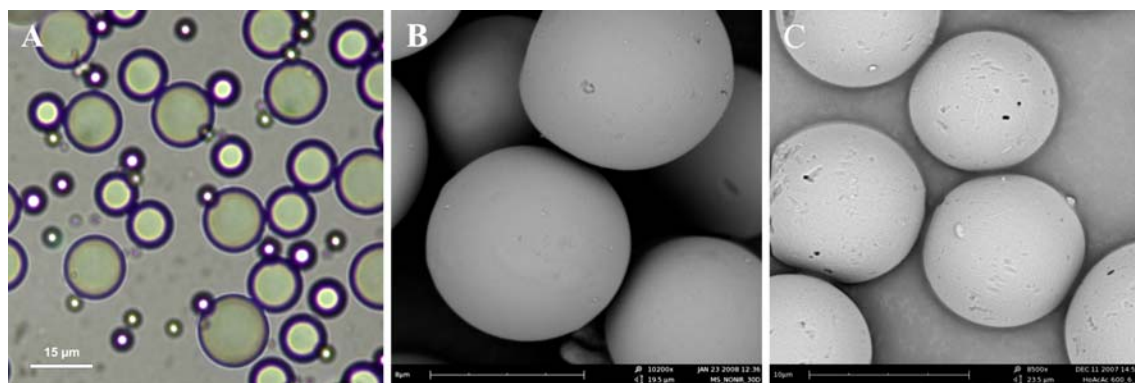


Fig. 1. A Light micrograph of HoAcAc microspheres before sieving (mean size 15 μm), B scanning electron micrograph of non activated HoAcAc microspheres and C scanning electron micrograph of HoAcAc microspheres after 6 h of neutron activation.

Table I. Calculated and Measured Elemental Composition of HoAcAc Crystals and Proposed and Measured Composition of HoAcAc Microspheres (in % *w/w*)

Element	HoAcAc Crystals $\text{Ho}(\text{AcAc})_3 \cdot 3\text{H}_2\text{O}$		HoAcAc Microspheres $\text{Ho}_2(\text{AcAc})_3 \cdot 4\text{H}_2\text{O}$	
	Calculated	Measured ^a	Proposed ^b	Measured
C	34.9	36.5	25.8	27.0
H	5.3	5.0	4.2	3.8
O	27.9	27.1	22.9	24.2
Ho	31.9	31.2	47.2	45.0

^a Data taken from Nijssen *et al.* (10)

^b Structure of HoAcAc microspheres is proposed based on measured elemental composition and Raman spectroscopy

distribution results, indicates that the microspheres are resistant to neutron irradiation.

The holmium content of the HoAcAc microspheres, as determined by complexometric titration, ICP OES and elemental analysis was found to be $45.0 \pm 0.5\%$ (*w/w*), which is significantly higher than the holmium content of the HoAcAc crystals, being 31.2% (*w/w*) (Table I). Also, the density of the HoAcAc microspheres (1.90 g/ml) was higher than the density reported for HoAcAc crystals (1.77 g/ml (20)). In the HoAcAc crystals, holmium is surrounded by three acetylacetonate ligands, and three water molecules (10,20). The increase in holmium content of the HoAcAc microspheres was explained by a loss of one or more acetylacetonate ligands caused by a structural rearrangement of the acetylacetonate ligands around holmium. This hypothesis was further investigated by determining the elemental composition of the microspheres and Raman spectroscopy.

The substantially higher holmium content per sphere (17.0% (*w/w*) for the HoPLLA microspheres *vs.* 45.0% (*w/w*) for the HoAcAc microspheres) results in a significant increase in radioactivity per sphere from 29 MBq/mg for HoPLLA microspheres (12) to 76 MBq/mg for HoAcAc microspheres (6 h neutron activation; thermal neutron flux of $5 \times 10^{12} \text{ n cm}^{-2} \text{ s}^{-1}$). Clinical results after intratumoral injection of ⁹⁰Y glass microspheres showed that 74 MBq ⁹⁰Y is sufficient to evoke a tumoricidal effect on a tumor of 3 cm (17). The injected volume of the microsphere suspension to such a tumor is limited to typically 0.1–0.3 ml (18). Based on the radiation characteristics of ¹⁶⁶Ho and ⁹⁰Y it can be calculated that a tumoricidal dose of ¹⁶⁶Ho activity (230 MBq/3 mg) can be delivered in this volume using HoAcAc microspheres for intratumoral administration (12).

Raman Spectroscopy

Infrared and Raman spectroscopy was performed to ascertain the presence of acetylacetonate in the microspheres. The Raman spectra of the HoAcAc crystals and the HoAcAc microspheres were virtually identical (Fig. 2), which implies that holmium is surrounded by acetylacetonate in both the HoAcAc crystals and the HoAcAc microspheres. These findings are in agreement with the infrared measurements on HoAcAc microspheres that showed the same peak characteristics as for HoAcAc crystals previously reported (21). The increase of the holmium content, found by elemental analysis, complexometric titration and ICP OES can therefore only be explained by a rearrangement of

acetylacetonate groups around the holmium(III) ion. Taking into account that holmium is surrounded by acetylacetonate ligands, and the results from the elemental analysis (Table I), we propose that per holmium ion one and a half acetylacetonate and two water molecules are present in the HoAcAc microspheres. The change of the acetylacetonate coordination should, in principle, be reflected in an intensity decrease of the Ho–O bending band, but since the position of this vibration is expected around 100 cm^{-1} (22), it is most likely filtered out with the Rayleigh scattering. The hypothesized structure of the HoAcAc microspheres is depicted in Fig. 3. As can be seen in this figure, acetylacetonate forms a bridge between two holmium(III) ions by coordinating each carbonyl to another holmium(III) ion forming a network. This bridging effect of chelates between metal ions has been proposed for metal catalysts after gradual removal of the solvent (23). The water observed in elemental analysis (Table I) is likely coordinated to the holmium(III) ion, as previously reported for HoAcAc crystals (20). An important observation that supports the network formation between holmium and acetylacetonate is that HoAcAc microspheres, in contrast to HoAcAc crystals, did not dissolve in chloroform.

Differential Scanning Calorimetry

The thermal behaviour of HoAcAc crystals and HoAcAc microspheres was investigated using modulated differential scanning calorimetry (mDSC). Representative mDSC scans of the holmium acetylacetonate crystals and microspheres are shown in Fig. 4, and relevant data are summa-

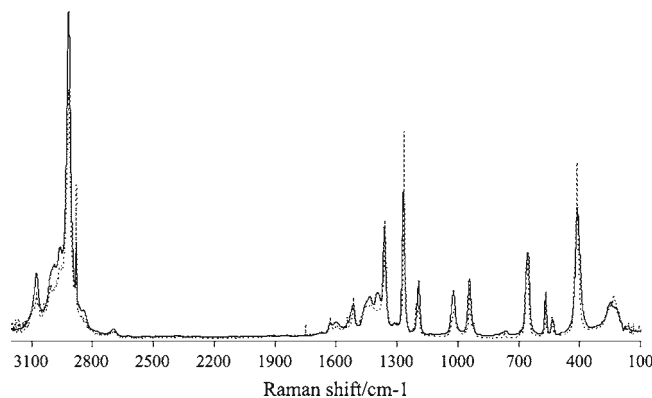


Fig. 2. Raman spectra of HoAcAc microspheres (solid line) and HoAcAc crystals (dotted line).

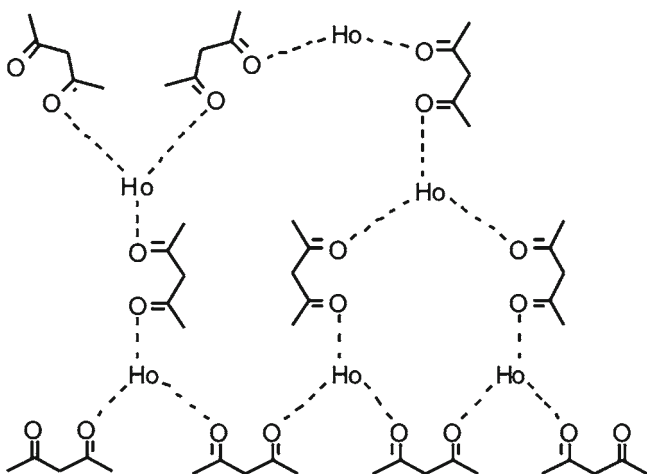


Fig. 3. The proposed interaction of acetylacetonate with holmium (III) ion in HoAcAc microspheres (coordinated water molecules not shown). Each acetylacetonate carbonyl oxygen coordinates with a separate holmium(III) ion, linking two holmium(III) ions.

ized in Table II. The thermogram for HoAcAc crystals shows an endotherm with a peak maximum at $123 \pm 7^\circ\text{C}$. This endotherm was ascribed to the loss of water from the complex, leading to the collapse of the crystalline structure of the crystals (21). HoAcAc microspheres show a distinctly different thermogram. We observed an endotherm at approximately $194 \pm 2^\circ\text{C}$, which is likely due to the loss of water from the structure. Interestingly, after heating to 200°C the microspheres were still intact, and the surface of the microspheres showed minor signs of damage. In contrast, heating of the HoAcAc crystals to 200°C lead to completely molten material, which is in agreement with literature (24). The resistance of microspheres to heating to 200°C is also an indication that a network is formed. Moreover, this resistance to heat allows for dry heat sterilization (25), making the microspheres suitable for *in vivo* use. DSC analysis of neutron activated HoAcAc microspheres showed an endotherm at $199 \pm 3^\circ\text{C}$, which is likely associated with the loss of water, which was also observed for the non activated microspheres.

X-ray Diffraction

The internal structure of the HoAcAc crystals and HoAcAc microspheres was studied using X-ray diffraction. The HoAcAc crystals have a crystalline structure (21), with a powder pattern reflecting the periodicity of the crystal

structure. The pattern for the HoAcAc microspheres shows no sharp peaks at a higher diffraction angle. This indicates the absence of repetitive intermolecular interactions, which is typical for amorphous structures. The broad peak in the HoAcAc microsphere diffraction pattern at a diffraction angle of approximately 11° can be attributed to the distance of two holmium atoms separated by one acetylacetonate molecule, which is approximately 4.5 \AA . Since holmium has a large scattering power due to the relatively high number of electrons, the high intensity peak at a diffraction angle of approximately 3.2° is ascribed to the Ho–Ho contact in its amorphous form, corresponding to a bond length of approximately 15.5 \AA (21).

Multimodality Imaging Characteristics

The paramagnetic nature and the high linear attenuation coefficient of holmium allows for multimodality imaging of non-radioactive HoPLLA microspheres.

To investigate if the multimodality imaging characteristics enhanced with an increase of the holmium concentration, the HoAcAc microspheres were homogeneously dispersed in an agarose gel matrix. The paramagnetic nature of holmium locally induces a magnetic field inhomogeneity, leading to an enhanced MRI signal decay in gradient echo images (13). The resulting r_2^* relaxivity of the HoAcAc microspheres with a holmium load of 45% (w/w), is $264 \pm 5.7 \text{ s}^{-1} \text{ mg}^{-1} \text{ ml}$, which is substantially higher than the r_2^* value for the HoPLLA microspheres with a holmium load of 17% (w/w) ($92 \pm 3.2 \text{ s}^{-1} \text{ mg}^{-1} \text{ ml}$) (26). This increase of the r_2^* relaxivity represents an enhanced sensitivity of MRI to the HoAcAc microspheres, as compared with HoPLLA microspheres, which can be explained by the increased holmium weight content per sphere.

Quantitative CT of the agarose phantom resulted in a mass attenuation coefficient at 120 kV of $15.6 \text{ HU mg}^{-1} \text{ ml}$ for HoAcAc MS, which is substantially increased, when compared to the mass attenuation coefficient of HoPLLA microspheres of $6.7 \text{ HU mg}^{-1} \text{ ml}$ at 120 kV (14). This increase in CT sensitivity, like the increase of sensitivity of MRI to the HoAcAc microspheres, can be attributed to the increase in holmium content.

To demonstrate the feasibility of visualization of microgram amounts of HoAcAc microspheres, using MRI and CT, decreasing amounts of HoAcAc microspheres (1 mg to 1 μg) in clusters were imaged *in vitro* as well as *ex-vivo*. The enhanced r_2^* relaxivity of the HoAcAc microspheres allowed for the detection of 1 μg of HoAcAc microspheres in the gel (Fig. 5A). The same setup was used for CT measurements, and the increased Ho content per sphere resulted in detection

Table II. Summary of DSC Data of HoAcAc Crystals and HoAcAc Microspheres Both Non Neutron Activated and Neutron Activated $n=6-8$

	Onset T_{max} ($^\circ\text{C}$) ^a	T_{max} ($^\circ\text{C}$) ^b	ΔH (J/g) ^c
HoAcAc Crystals	118 ± 7	123 ± 7	115 ± 9
HoAcAc Microspheres	188 ± 2	194 ± 2	25 ± 5
Neutron activated HoAcAc Microspheres	190 ± 3	199 ± 3	12 ± 11

^a Onset T_{max} : onset of the endotherm

^b T_{max} : peak maximum of the endotherm

^c ΔH : enthalpy of the endotherm

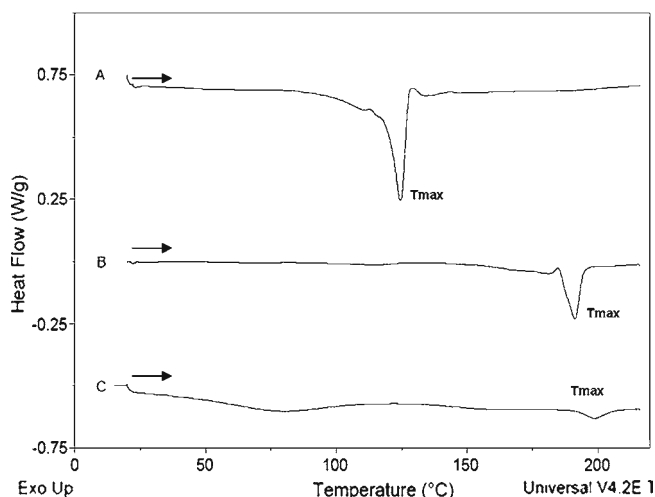


Fig. 4. mDSC thermograms of **A** holmium acetylacetonate crystals, **B** holmium acetylacetonate microspheres and **C** neutron activated (6 h) holmium acetylacetonate microspheres. T_{max} is the maximum peak of the endotherm.

of 50 μg HoAcAc microspheres (Fig. 5B and C). We used an excised rabbit liver (Fig. 5D), with depots of 1, 5 and 10 μg HoAcAc microspheres to investigate the *ex-vivo* imaging characteristics on MRI. The inhomogeneity of the *ex-vivo* rabbit liver resulted in the detection of depots from 5 μg onwards (Fig. 5E and F).

Unlike the ^{90}Y microspheres, which lack the MR imaging possibilities, holmium microspheres can be visualized directly therefore allow for tracking of the microspheres long after the radioactive ^{166}Ho has decayed, and thus establish the *in vivo* fate of the microspheres after intratumoral injection in a non invasive manner using MRI. The detection of microgram amounts of HoAcAc microspheres will also enable MRI guided administration of the particles, allowing for accurate positioning of the depots in tumor tissue, whilst refraining healthy tissue from radiation damage.

Clinical Perspective

The two currently available ^{90}Y microspheres are glass-based (Therasphere®, MDS Nordion, Kanata, Canada) or resin-based (SIR-Spheres®, SIRTex Medical Ltd., Sydney, Australia). The glass microspheres have a very high specific activity (2.5 kBq/microsphere), and are registered as a Humanitarian Use Device by the FDA for use in radiation treatment or neoadjuvant to surgery or transplantation in patients with unresectable hepatocellular carcinoma (27). The resin based microspheres have a relatively low specific activity 40 Bq/sphere, and were granted premarket approval by the FDA in 2002 (27).

With regard to the transcatheter approach, the HoAcAc microspheres might be considered for treatment of patients with hypovascular liver malignancies. This is due to the specific activity of the $^{166}\text{HoAcAc}$ microspheres which is in

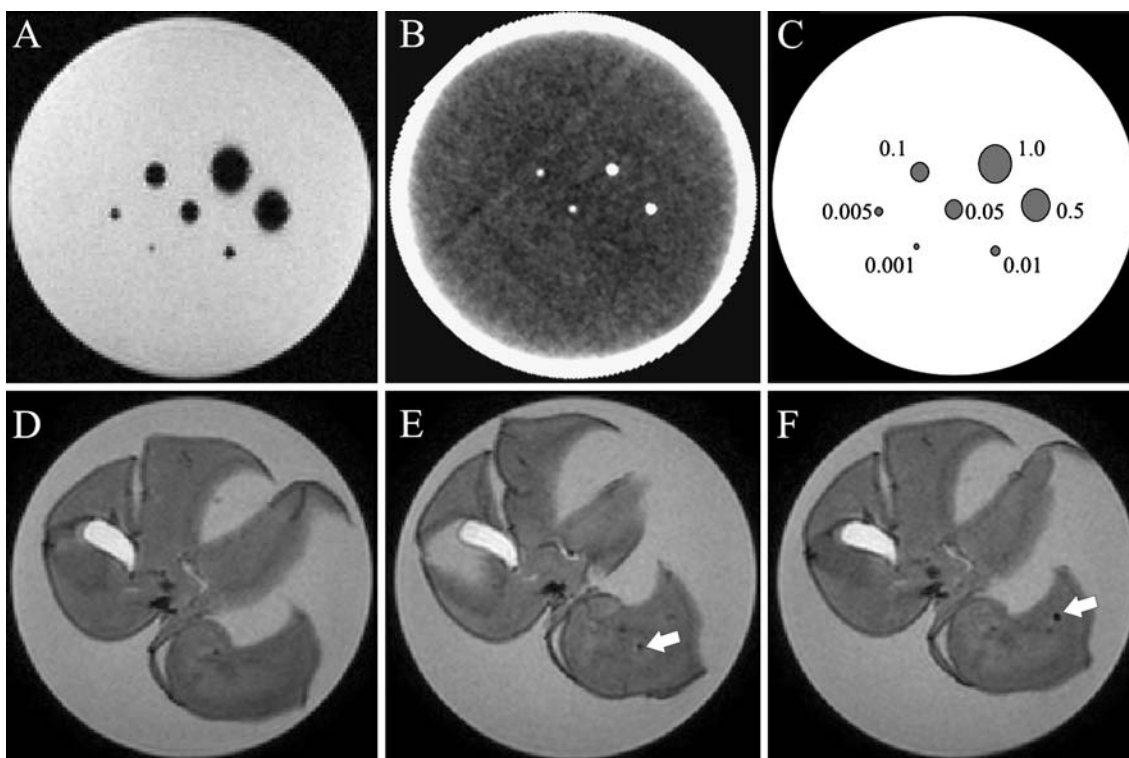


Fig. 5. **A** Gradient echo MRI image of agarose phantom with different depots of HoAcAc microspheres, **B** CT image of agarose phantom with different depots of HoAcAc microspheres, **C** schematic representation of agarose phantom with different depots of HoAcAc microspheres, including the amount of microspheres in milligram, **D** MRI image of rabbit liver before administration of HoAcAc microspheres, **E** MRI image of rabbit liver after administration of 5 μg HoAcAc microspheres, indicated by arrow, **F** MRI image of rabbit liver after administration of 10 μg HoAcAc microspheres, indicated by arrow.

the range of the specific activity of the glass ^{90}Y microspheres. The obvious advantage of the $^{166}\text{HoAcAc}$ microspheres lies in multimodality imaging.

Moreover, the high specific activity of the $^{166}\text{HoAcAc}$ microspheres will allow for the delivery of a tumoricidal dose through intratumoral injections. This approach is thought to be applicable not only in patients with liver malignancies, but also in patients with solid tumors in other organs, e.g. brain, kidney and lungs.

However, before a phase I clinical study is allowed to be conducted, several issues need to be addressed. First the pharmaceutical quality needs to be investigated, e.g. stability testing. Secondly, the *in vivo* toxicity needs to be assessed. The toxicity is expected to be minor, since holmium is a relatively non toxic metal (28). Finally, the therapeutic efficacy of the $^{166}\text{HoAcAc}$ microspheres needs to be evaluated in tumor bearing animals.

CONCLUSION

In conclusion, the present study demonstrates that microspheres with an ultra high holmium content can be prepared from HoAcAc crystals as the sole starting material, without the use of a polymeric matrix, using a solvent evaporation process. The resulting microspheres have a smooth surface, and are resistant to neutron activation with a thermal neutron flux ($5 \times 10^{12} \text{ n cm}^{-2} \text{ s}^{-1}$) and heating to 200°C. The mean particle size can be tailored for different tumor treatment approaches by adapting the processing parameters. The size increased from 15 to 26 μm when lowering the stirring rate from 500 to 300 rpm during emulsifying. The HoAcAc microspheres have an unexpectedly high holmium content of 45% (*w/w*) which is substantially higher when compared to the HoPLLA microspheres (17% (*w/w*)). Moreover, the holmium content in HoAcAc microspheres is higher than in the HoAcAc crystals (31% (*w/w*)), which is attributed to a rearrangement of acetylacetonate molecules around the holmium(III) ion, resulting in the loss of one and a half coordinating acetylacetonate molecules per holmium(III) ion. The data of this study suggest that acetylacetonate acts as a bridge between holmium(III) ions, forming an amorphous network. The increased holmium content leads to a 2.6 fold higher radioactivity per sphere (29 MBq/mg for HoPLLA microspheres vs. 76 MBq/mg for HoAcAc microspheres), which allows for tumoricidal radioactive doses in small volumes necessary for direct intratumoral injection. Additionally, the increased holmium content leads to a higher sensitivity for MRI and CT imaging, enabling detection of microgram amounts of microspheres *in vivo*.

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